Non-invasive, non-radiological quantification of anteroposterior knee joint ligamentous laxity
A STUDY IN CADAVERS

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Objectives
We performed in vitro validation of a non-invasive skin-mounted system that could allow quantification of anteroposterior (AP) laxity in the outpatient setting.

Methods
A total of 12 cadaveric lower limbs were tested with a commercial image-free navigation system using trackers secured by bone screws. We then tested a non-invasive fabric-strap system. The lower limb was secured at 10° intervals from 0° to 60° of knee flexion and 100 N of force was applied perpendicular to the tibia. Acceptable coefficient of repeatability (CR) and limits of agreement (LOA) of 3 mm were set based on diagnostic criteria for anterior cruciate ligament (ACL) insufficiency.

Results
Reliability and precision within the individual invasive and non-invasive systems was acceptable throughout the range of flexion tested (intra-class correlation coefficient 0.88, CR 1.6 mm). Agreement between the two systems was acceptable measuring AP laxity between full extension and 40° knee flexion (LOA 2.9 mm). Beyond 40° of flexion, agreement between the systems was unacceptable (LOA > 3 mm).

Conclusions
These results indicate that from full knee extension to 40° flexion, non-invasive navigation-based quantification of AP tibial translation is as accurate as the standard validated commercial system, particularly in the clinically and functionally important range of 20° to 30° knee flexion. This could be useful in diagnosis and post-operative evaluation of ACL pathology.

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Keywords: Non-invasive, Anterior cruciate ligament, Cadaveric, Precision, Accuracy, In vitro, ACL, Laxity

Article focus
Non-invasive adaptation of computer navigation technology is as reliable, precise and accurate as a commercially available, image-free, invasive navigation system

Key messages
From extension to 40° of knee flexion the non-invasive method is as reliable, precise and accurate as the commercial invasive system
Beyond 40° knee flexion, reliability and accuracy are unacceptable

Strengths and limitations
This is the first validation of a non-invasive adaptation of navigation-based technology that uses similar frames of reference to those used intra-operatively in measuring anteroposterior tibial translation
These data provide a foundation and rationale for further in vivo analysis
A limitation of this study is the use of cadaveric material, which was mandatory given the nature of the invasive comparison. Further in vivo validation must now be performed before the device is used in in vivo research or clinical practice

Introduction
Evaluation of anterior cruciate ligament integrity in the clinical setting relies predominantly on establishing anteroposterior (AP) laxity by manual testing. The Lachman test
has been shown to be highly sensitive in the diagnosis of cruciate deficiency,1,5 but in terms of evaluating cruciate ligament reconstruction, the test remains examiner-dependent and subjective. The reliability of non-invasive methods that objectively evaluate AP translation is reported as inconsistent in the literature.5,15

Image-free navigation has been thoroughly validated and is used by many surgeons to provide intra-operative assessment of AP tibial laxity.16–19 The role of this technology is limited to the operative setting due to the requirement for invasive optical tracker placement. A non-invasive adaptation of this technology using software algorithms identical to those used in a commercially available image-free navigation system has been validated to quantify lower limb mechanical and coronal knee laxity in early flexion.20,21 Using the same fabric strap method, a pilot study on six embalmed cadaveric lower limbs gave acceptable reliability, precision and agreement with a conventional image-free navigation system measuring AP translation in early flexion.22

The primary aim of this study was to compare a non-invasive system with a validated and commonly used intra-operative computer navigation system in terms of reliability and repeatability of AP translation measurement and agreement with the invasive system. The secondary aim was to observe the effect of knee flexion on measurement reliability, precision and agreement between the two systems.

Materials and Methods
A single investigator (DFR) carried out all testing. A total of 12 lower limbs were used from eight cadavers (five female and three male, mean age 80.5 years (65 to 91)). The image-free OrthoPilot navigation system was used with passive optical trackers (B. Braun Aesculap, Tuttingen, Germany). The optical camera was positioned 2 m from the specimen. Experimental software allowed registration of the centres of the hip, knee and ankle following a series of prescribed lower limb movements and localisation of key bony landmarks. The registration algorithms in this software are identical to validated, commercially available software used in computer-assisted surgery.

Two separate methods of tracker fixation were used: standard bone screws with tracker mounts, and a fabric strap used to secure a baseplate. The fabric strap and baseplate used in this study had been validated.20 In order to allow attachment of a transducer to the anterior tubia to allow application of a moment perpendicular to the coronal plane of the tibia, a screw with eyelet was inserted into the tibial tuberosity. A 3 cm incision was made over the proximal anterior femur down to bone and all soft tissues were cleared from the anterior femoral cortex. Both cortices were drilled and a screw with an eyelet inserted perpendicular to the long axis of the femur. This screw was used to suspend the thigh above the laboratory table, thus minimising soft-tissue artefacts from the work-surface. In order to create a foot support, a loop of cord from a second laboratory stand was secured proximal to the metatarsal heads; this maintained the angle of flexion of the knee. In order to limit knee extension during testing, four separate bungee cords were attached to two screws inserted into the medial and lateral distal tibial cortices. These cords were secured to the laboratory table. Various lengths were available and changed to adapt to various positions of knee flexion, keeping the bungee cords as tight as possible according to position of the foot throughout range of knee flexion. The pull of the bungee cord was counteracted by the foot support, resulting in no flexion or extension of the knee joint during AP tibial stress testing.

The limbs were put through 24 full cycles of flexion and extension and ten applications of 100 N anterior force applied via the tibial tuberosity screw before testing in order to minimise systematic error due to progression of tissue elasticity. The experiments were carried out over 12 days, during which the temperature of the laboratory was controlled and constant. The specimens were not refrigerated between experiments.

AP tibial translation was recorded by the system following force application at intervals of 10° from extension to 60° of knee flexion. This procedure was performed twice using optical trackers mounted invasively using bone screws, and twice using the non-invasive fabric strap method. A force transducer was secured to the tibial tuberosity eyelet screw and a linear force applied in an anterior direction perpendicular to the long axis of the tibia until a force of 100 N had been reached. The value of 100 N was selected considering various methodologies used in previous in vitro and in vivo testing of AP laxity of the knee joint.6,7,10,23,24 The software automatically recorded maximum displacement in millimetres. The investigator did not watch the computer monitor during testing – however, true blinding to results throughout the entire experiment was not possible due to single investigator setup and potential contamination issues while handling fresh cadaveric material. Only the foot pedal could be accessed during testing and the screen could not be repeatedly obscured between tests.

Statistical analysis. Statistical testing was applied to measurements taken from each interval of 10° flexion separately to allow analysis of the effect of knee flexion angle on reliability, repeatability and agreement. Reliability within each method of tracker fixation used in measuring AP tibial translation was analysed by calculating the intraclass correlation coefficients (ICCs).25 A coefficient of ≥ 0.75 demonstrates very good reliability.26,27 The calculation of ICC was performed using IBM SPSS v17.0 software (IBM Corp., Armonk, New York). Coefficient of repeatability (CR) was calculated to demonstrate repeatability between test–retest measurements within each method of tracker fixation.28 The CR defines the interval within which 95% of test–retest
differences lie (i.e. within 2 SDs of the test–retest differences). A limit of 3 mm was chosen for the repeatability of measurements when considering each system separately, and as a limit for agreement margin between the systems. This value was chosen based on diagnostic criteria for dichotomous testing between ‘normal’ and ‘injured’ knees when testing for ACL insufficiency using other measurement devices. A CR ≤ 3 mm denotes that 95% of all measurements are within a range of ±1.5 mm.

Bland–Altman plots were generated as a visual representation of the limits of agreement. 95% limits of agreement (LOA) were determined using the corrected standard deviation of the differences (SDc) to allow for repeated measurements. Mean difference between the system measurements ±1.96 SDc reflects the limits of agreement between the two systems. Acceptable limits of agreement were once again set at 3 mm. CR and LOA calculations were performed using Microsoft Excel (Microsoft Corp., Redmond, Washington).

Results

The mean fixed flexion for the 12 specimens was 6.8° (0° to 15°).

Figure 1 demonstrates the mean CR at each flexion interval throughout the range of flexion tested in this experiment (12.8° to 60°). Bland–Altman plots demonstrated no systematic error plotting screw fixation versus fabric strap fixation (Fig. 2). Figure 3 displays LOA at each 10° interval of knee flexion between measurements taken using invasive versus non-invasive tracker mounting.

It was noted during the experiment that despite obvious subjective AP movement of the tibia, the system measured ‘0 mm’ AP displacement. This occurred at higher angles of flexion only, during one test at 50° flexion and during six tests at 60° flexion using the invasive and non-invasive methods.

Discussion

From extension to 40° knee flexion, both devices displayed similarly good reliability and precision. In this range, agreement between the devices is also acceptable. The angle of knee flexion does not affect precision, but it does affect accuracy of the non-invasive method in flexion > 40°. The validity of this non-invasive device has been demonstrated in the in vitro setting as it has demonstrated acceptable reliability, precision and accuracy between extension and 40°. Additional in vivo work should be carried out to further validate the device, as this range of knee flexion permits important tests of knee laxity such as the Lachman test, and is a useful range for demonstrating dynamic weight-bearing stability in early flexion such as squatting, ascending or descending a step when patients with ACL insufficiency often report feelings of ‘giving way’.

Limitations of this experiment include use of cadaveric tissue, which lacks muscle tone and has different tissue properties to the in vivo setting. The invasive nature of the validation methodology used in this experiment mandated the use of cadaveric limbs. However, it is now important to study the effect on the non-invasive system.
of artefacts from live soft tissue in a range of live subjects. The experiment set-up involving limb suspension and securing knee flexion angle will alter kinematics of the lower limb to some degree. However, this set-up provided consistent testing conditions in terms of joint positioning, removing variables that may have obscured testing of precision and accuracy. These limitations are characteristic to in vitro validation of clinical devices and such experimental work is very important before progressing to reliability testing in vivo, in which the comparison of kinematic measurement is either not attempted or involves consequential intervention such as invasive placement of markers or ionising radiation. Based on the results of this study, in vivo validation should now be carried out. A limitation common to all image-free navigation systems is a decrease in accuracy beyond 50° of knee flexion, which is well documented in the literature. This is due to the femoral frame being defined by the transepicondylar axis (TEA), the landmarks for which are acquired at registration. The TEA collected at registration is not accurate enough to compensate for the marked displacement of the femoral and tibial axes during high knee flexion. This phenomenon was observed at higher flexion angles in this study. The limitation beyond 50° of knee flexion is important to note when using image-free navigation in any setting.

From extension to 40° flexion, the results of reliability, precision and accuracy are favourable for the non-invasive method of tracker fixation compared with arthrometric devices. Generally these devices provide a reliability (ICC) of 0.6. Concerns have been raised over accuracy of the most popular clinical devices, such as the KT-1000 (MEDmetric Corporation, San Diego, California). AP rather than rotatory laxity is the most reliable kinematic indicator of cruciate ligament integrity. Increases in anterior translation of between 2 mm and 14.4 mm following sectioning of the ACL have been reported using various methods of force application and measurement. Isberg et al compared normal knees with those with ACL rupture in 22 patients using radiostereometric analysis, and found a mean difference in anterior translation of 7.4 mm (2.2 to 17.4). Sectioning of the ACL has been shown in biomechanical studies to increase internal rotation by only 2° to 4° with the knee in early flexion (i.e., 20° to 30°). The posterior cruciate ligament is even less involved in rotatory stability, only demonstrating significant effect at 90° of knee flexion. Furthermore, reconstruction of the ACL may not restore rotational kinematics. Non-invasive devices assessing tibial rotation with an aim of detecting cruciate ligament pathology or dysfunction would have to be very sensitive compared with those detecting AP instability. The reliability of current devices used to quantify rotational laxity is relatively low and such devices are not routinely used in clinical practice, with the vast majority still in pre-clinical development. The pivot shift phenomenon has been mapped and characterised using invasive navigation-based technology, allowing comparison of ACL reconstruction techniques. However, a non-invasive adaptation of this has not yet tested in the clinical setting. Until more sensitive means of analysing tibial rotation are available, it may be more useful to detect AP instability for diagnosis of cruciate pathology and evaluation of surgical reconstruction.

Should the non-invasive method of tracker fixation method prove valid in vivo, it would provide a useful adjunct to clinical examination aiding diagnosis of cruciate pathology. A method of quantifying the forces applied during examination would increase knowledge of ‘normal’ laxity, allow standardisation of examination technique and permit comparison of surgical results between practitioners.

**Conclusion.** In the in vitro setting, the non-invasive method of tracker fixation proved as reliable and precise as the invasive method in measuring AP tibial translation, and demonstrated acceptable agreement within a diagnostically applicable range from full knee extension to 40° knee flexion.

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**References**


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Author contributions:
- D. E. Russell: Design of the experimental set-up, Data collection, Data analysis, Writing the paper
- A. H. Deakin: Study design, Data analysis, Writing the paper
- Q. A. Fogg: Supervision of design of experimental set-up, Data collection, Review of manuscript
- F. Picard: Study concept, Study design, Review of data analysis, Review and editing of manuscript

ICMJE Conflict of Interest:
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